Background: A new commercially available device (IOLMaster, Carl Zeiss Jena GmbH) provides high resolution non-contact measurements of axial length (using partial coherent interferometry), anterior chamber depth, and corneal radius (using image analysis). The study evaluates the validity and repeatability of these measurements and compares the findings with those obtained from instrument currently used in clinical practice.

Method: Measurements were taken on 52 subjects (104 eyes) aged 18–40 years with a range of mean spherical refractive error from +7.0 D to −9.50 D. IOLMaster measurements of anterior chamber depth and axial length were compared with A-scan applanation ultrasonography (Storz Omega) and those for corneal radius with a Javal-Schötz keratometer (Topcon) and an EyeSys corneal videokeratoscope.

Results: Axial length: the difference between IOLMaster and ultrasound measures was insignificant (0.02 (SD 0.32) mm, p = 0.47) with no bias across the range sampled (22.40–27.99 mm). Anterior chamber depth: significantly shorter depths than ultrasound were found with the IOLMaster (−0.06 (0.25) mm, p < 0.02) with no bias across the range sampled (2.85–4.40 mm). Corneal radius: IOLMaster measurements matched more closely those of the keratometer than those of the videokeratoscope [mean difference −0.03 v −0.06 mm respectively], but were more variable (95% confidence 0.13 v 0.07 mm). The repeatability of all the above IOLMaster biometric measures was found to be of a high order with no significant bias across the measurement ranges sampled.

Conclusions: The validity and repeatability of measurements provided by the IOLMaster will augment future studies in ocular biometry.

Materials and Methods
Fifty two subjects (32 male and 20 female), with a mean age of 25.2 (SD 4.7) years (range 18–40 years, median 23.6 years) participated in the study. Subjects with ocular pathologies, abnormal binocular vision, and previous allergy to the topical anaesthetic benoxinate hydrochloride were excluded from the study. Measurements were performed on 104 eyes by two qualified optometrists (JS-R and EAHM), after the purpose of the study was explained and informed consent given. The monitor of the instrument was used to align the right eye, followed by the left, with the instrument’s internal fixation target. The eyes were in focus when the instrument head was approximately 5.5 cm away from the subject’s eyes. Subjects were asked to perform a complete blink just before measurements were taken in order to spread an optically smooth tear film over the cornea.

Corneal curvature was measured with the IOLMaster and compared with measures from a videokeratoscope (EyeSys Instruments, Houston, TX, USA) and a Javal-Schötz keratometer (Topcon, Capelle a/d IJssel, Netherlands). The IOLMaster reflects six points of light, arranged in a 2.3 mm diameter hexagonal pattern (measured by digital callipers), from the air/tear film interface. The separation of opposite pairs of lights is measured objectively by the instrument’s internal fixation target. The eyes were in focus when the instrument head was approximately 5.5 cm away from the subject’s eyes. Subjects were asked to perform a complete blink just before measurements were taken in order to spread an optically smooth tear film over the cornea.

Corneal curvature was measured with the IOLMaster and compared with measures from a videokeratoscope (EyeSys Instruments, Houston, TX, USA) and a Javal-Schötz keratometer (Topcon, Capelle a/d IJssel, Netherlands). The IOLMaster reflects six points of light, arranged in a 2.3 mm diameter hexagonal pattern (measured by digital callipers), from the air/tear film interface. The separation of opposite pairs of lights is measured objectively by the instrument’s internal fixation target. The eyes were in focus when the instrument head was approximately 5.5 cm away from the subject’s eyes. Subjects were asked to perform a complete blink just before measurements were taken in order to spread an optically smooth tear film over the cornea.

Materials and Methods

Fifty two subjects (32 male and 20 female), with a mean age of 25.2 (SD 4.7) years (range 18–40 years, median 23.6 years)
Anterior chamber depth was measured with the IOLMaster and compared with measures from an A-scan applanation ultrasound device (Storz Omega Compu-Scan Biometric Ruler, Storz International, St Louis, MO, USA). The IOLMaster directs a 0.7 mm width slit beam of light through the anterior segment of the eye at an angle of 38 degrees to the visual axis. The instrument camera is aligned so that the light beam forms an optical section and the internal software measures the distance between the anterior corneal pole and the anterior crystalline lens surface to calculate the anterior chamber depth. The A-scan applanation device calculates anterior chamber depth from the time taken for ultrasound waves to reflect back to its receiver from an optical surface. One drop of topical anaesthetic, benoxinate hydrochloride 0.4% (Minims, Chauvin Pharmaceuticals Ltd), was instilled in each of the subject’s eyes 2 minutes before ultrasound measurement. Special care was taken in aligning the transducer beam probe along the optical axis and to exert minimal corneal pressure. Ten measurements were taken for each eye and the mean calculated.

Axial length was measured with the IOLMaster and compared with measures from the A-scan applanation ultrasound device. The IOLMaster measures optical axial length by partial coherence interferometry, based on the Michelson interferometer (Fig 1). The laser diode (LD) generates infrared light (\( \lambda = 780 \, \text{µm} \)) of short coherence length (\( C_c = 160 \, \text{µm} \)), which is reflected into the eye by mirrors M1 and M2, after being split into two equal coaxial beams CB1 and CB2 by the beam splitter B1. The separation of the two coaxial beams is twice the displacement \( d \) of the mirror M1. Both coaxial beams enter the eye, where reflections take place at the corneal (C) and retinal (R) interfaces. On leaving the eye, the difference in frequency between the coaxial beams is detected by a photodetector (PHD), allowing accurate measurements of the length \( AL \) between the cornea and the retina. Measurements with this device are not affected by longitudinal eye motion. The calculation of axial length is dependent on the refractive index of the medium in which the light travels, and therefore the optical path length is divided by the mean group refractive index (taken as \( n = 1.3549 \)) in order to obtain the geometrical axial length. Laser light is reflected from the retinal pigment epithelium, in contrast with ultrasound waves which are reflected from the internal limiting membrane. Hence, in order to make the IOLMaster results comparable with previous ultrasound measures, a conversion factor has been incorporated into the instrument software. The A-scan applanation device calculates axial length from the time taken for ultrasound waves to reflect back to its receiver from the internal limiting membrane. Three separate measurements were recorded for both axial length and corneal curvature, whereas a single shot automatically generated five measures of anterior chamber depth. In around 5% of subjects, measurements were automatically rejected by the instrument as, compared with the respective mean, they were different by 0.05 mm for corneal curvature, 0.15 mm for anterior chamber depth or the signal to noise ratio (an indicator of measurement quality) for axial length was lower than 2.0. In these cases, an error message was displayed on the monitor and the measure repeated.

Objective refraction was performed with the Shin-Nippon SRW-5000 autorefractor and the mean spherical equivalent calculated from six readings. The repeatability of the IOLMaster was examined by measuring corneal curvature, anterior chamber depth, and axial length on the same subjects after a period of 1–10 days from the initial measurement.

Statistical analysis

The bias between measures (the mean difference, standard deviation, and 95% confidence limits) was calculated and presented graphically. Comparison between measures was performed using paired two tailed \( t \) tests. Corneal curvatures
were converted from dioptres into a vector representation in millimetres for analysis: a spherical lens of power MSE (the mean spherical equivalent = sphere + [cylinder/2]); Jackson cross cylinder at axis 0° with power J0 (= −[cylinder/2] cos[2 × axis]); Jackson cross cylinder at axis 45° with power J45 (= −[cylinder/2] sin[2 × axis]). The level of agreement between biometry measures and ocular refraction was tested using the Pearson’s product moment correlation coefficient.

RESULTS

Corneal curvature measurement differences between the IOL-Master, Javal-Schiötz keratometer, and videokeratoscope are shown in Table 1. The mean difference in corneal curvature measured by the IOL-Master was in better agreement with the Javal-Schiötz keratometer than the videokeratoscope, but more variable (Fig 2). The broken lines on the graphs (Figs 2–4) indicate the extent to which the IOL-Master might over-read or under-read compared to the alternative methods examined (that is, the IOL-Master could be expected to read as much as 0.01 mm above or 0.13 mm below the corneal videokeratoscope for mean corneal curvature).

Anterior chamber depth, as measured with the IOL-Master, was significantly shorter (by −0.06 (0.25) mm, p <0.02) than that measured by applanation ultrasound (Fig 3). There was no significant mean difference (bias) in the accuracy of the instrument for the whole range of anterior chamber depths evident in this study (that is, 2.85–4.40 mm). The IOL-Master could be expected to read as much as 0.01 mm above or 0.07 mm below ultrasound for anterior chamber depth.

Axial length, as measured with the IOL-Master, was similar to that measured by applanation ultrasound (difference 0.02 (0.32) mm, p = 0.47; Fig 4). Again, there was no significant bias in the accuracy of the instrument for the whole range of axial lengths evident in this study (that is, 22.40–27.99 mm). The IOL-Master could be expected to read as much as 0.05 mm above or 0.61 mm below ultrasound for axial length.

The repeatability of corneal curvature measurements repeated after an interval of between 1 and 10 days is given in Table 2. The mean difference in anterior chamber depth (−0.01 (0.08) mm, p = 0.24; Fig 3) and axial length (0.00 (0.04) mm, p = 0.75; Fig 4) measured with the IOL-Master was insignificant and there was no bias over the whole range. A significant correlation with ocular refraction was found for anterior chamber depth (r = 0.51, p <0.01) and axial length (r = −0.77, p <0.01).

DISCUSSION

The study shows that the validity, repeatability, and clinical utility of optical and image analysis methods of assessing ocular biometric measures, match at least those offered by...
instrumentation currently used in clinical practice and it is envisaged that the IOLMaster will be well received in both the clinical and research environment.

**Validity**

The close match found between axial length measurements using the IOLMaster and applanation ultrasound (0.02 (0.32) mm) is consistent with those reported previously by Hitzenberger, who found a difference between Doppler interferometry and water immersion ultrasonography of 0.01 (0.13) mm. This study has found a closer agreement between PCI and applanation ultrasonography than most of the previous reports. The IOLMaster image analysis procedure for measuring anterior chamber depth gave values that closely matched those for applanation ultrasound. Although there was a statistically significant difference between these measurements (on average ~0.06 mm), this is smaller than the resolution of applanation ultrasound and clinically insignificant (<2% of the anterior chamber depth). IOLMaster measures of corneal curvature were similar to those of keratometry and videokeratoscopy.

**Repeatability**

The coefficient of repeatability for IOLMaster axial length measurements found in this study (0.00 (0.04) mm) is clearly impressive when compared with those generally found for ultrasound, in which a difference between the first and the mean of three or five readings has been found to be of the order of 0.1 to 0.15 mm. Previous studies using optical methods have used the mean standard deviation of single session measurements found in this study (0.00 (0.04) mm) is clearly repeatable, high resolution measurements of axial length. IOLMaster measures of corneal curvature had repeatability levels similar to those previously reported for keratometry and videokeratoscopy.

**Clinical utility**

The facility for taking biometry measurements without the need for corneal contact is a particular advantage in both clinical and research environments and especially in child studies as, once fixation has been achieved, it is claimed that only 0.5 seconds is required to perform a measurement. The significant correlation between axial length and ocular refraction reported in this study is well documented. In contrast, a weaker, but significant, correlation was found between anterior chamber depth and ocular refraction. Previous studies have failed to support this latter finding. The IOLMaster currently cannot provide measures of lens thickness but, despite this, its higher level of precision and repeatability for anterior chamber depth may provide further insight into the role of anterior segment dimensions in emmetropisation. Drexler and colleagues have developed a non-commercial instrument which uses PCI to measure lens thickness with a precision of 8–10 µm and a resolution of 9 µm and is thus able to monitor temporal change in the accommodation response, but the wavelength of laser light used cannot penetrate the eye as far as the posterior pole for concomitant measures of axial length. Accurate axial length determination is also of particular relevance in the quantitative analysis of fundus structures such as the optic disc, the neuroretinal rim area, and the retinal nerve fibre layer thickness. Determination of retinal contour is relevant to our understanding of the mechanisms of eye growth. Previous studies have determined retinal contour using relatively complex computer software analysis which requires input data obtained from A-scan ultrasonography, keratometry, and peripheral refraction. Determination of retinal contour with PCI methods has been previously reported for a single individual and represents a valuable facility for future studies on posterior segment dimensions. The axial length:corneal radius ratio has been proposed as a biometric predictor for the onset and development of myopia, particularly in children. Examination of the utility of this ratio will be enhanced by the ability of the IOLMaster to provide non-contact, successive, repeatable, high resolution measurements of axial length and corneal radius.

**References**


The authors have no proprietary interest in the IOLMaster.


